

# An in-vitro test for the duration of action of insulin suspensions

D. T. GRAHAM\* AND A. R. POMEROY

*Pharmacology Section, National Biological Standards Laboratory, Canberra, A.C.T., Australia*

A method is described which measures the prolongation effects of commercial insulin suspensions by monitoring the rate of solution of an insulin suspension into a phosphate buffer, pH 7.4, at 37°C. The method can rapidly categorize an insulin into the clinical classifications of either fast, intermediate or slow acting. It offers advantages of speed and sensitivity over the British Pharmacopoeial test for prolongation of insulin effect in fasted animals. Large differences between the dissolution rates of commercial samples of isophane insulin were observed which suggested a lack of bioequivalence.

Insulin preparations are often classified according to their clinical duration of action: fast acting, intermediate acting and slow acting (Larner 1980). Commercial injections of insulin suspensions are tested for their duration of action using the Prolongation of Insulin Effect as described in the British Pharmacopoeia 1980 (BP). This test compares the hypoglycaemic effects of an insulin suspension with those of a standard insulin solution following subcutaneous injection into fasting animals. However, the test is unreliable because the changes in the blood sugar levels in response to a given dose of insulin can vary markedly between animals, and the test does not incorporate a cross-over design. This variability is compounded by the inaccuracies involved in injecting a few µlitres of an insulin suspension subcutaneously. An alternative in-vitro procedure to monitor the dissolution characteristics of commercial insulin suspensions is described. The procedure involves continuously measuring the rate of dissolution of insulin particles into a phosphate buffer at 37°C.

## MATERIALS AND METHODS

### *In-vitro dissolution method*

Two ml of insulin suspension, 100 U ml<sup>-1</sup>, is placed in a 25 mm Millipore ultrafiltration cell containing a magnetic stirrer. The suspension is filtered through a 0.22 µm membrane filter under positive pressure and the trapped particles washed with 1 ml of cold distilled water, and adjusted to pH 7.0, to remove any preservatives. Sorensen's phosphate buffer, 0.067 M, pH 7.4, warmed to 37°C, is pumped through the cell at a rate of 3 ml min<sup>-1</sup> from a 200 ml

reservoir stirred with a magnetic stirrer. The absorbance of the filtrate is continuously measured at 214 nm by a Varian spectrophotometer as it passes through a flow cell, and then back to the reservoir. The stirring rate in the ultrafiltration cell is 120 rev min<sup>-1</sup>. Duplicate curves are obtained for each product. (If the phosphate buffer is replaced with 0.14% sodium acetate, pH 7.1, minimal dissolution occurs and there is no differentiation between formulations.)

### *In-vivo prolongation of insulin effect*

The procedure of the BP was followed, using 9 rabbits per group. Each rabbit received insulin 0.5 U kg<sup>-1</sup> and whole blood sugar levels were measured by a method based on that of Hoffman (1937), using a Technicon Auto-Analyser.

### *Products*

Samples of commercial insulin injections, 100 U ml in 10 ml, manufactured and/or distributed by Boots, the Commonwealth Serum Laboratory, Nordisk, Novo, Weddel and Wellcome were used. The insulin formulations tested were the slow acting preparations, protamine zinc insulin and insulin zinc suspension crystalline; the intermediate acting insulins, isophane insulin and insulin zinc suspension mixed; and the fast acting insulin, insulin zinc suspension amorphous. All products complied with the relevant requirements of the BP 1980.

## RESULTS

Dissolution curves were obtained for several types of insulin suspensions by continuously measuring the light absorbance caused by insulin dissolved in the filtrate, against elapsed time. Initial studies showed

\* Correspondence.

that the phosphate buffer volume did not limit the solubility of the insulin crystals, since the absorbance increased or decreased inversely with buffer volumes. Similarly, small changes (90–150 rev min<sup>-1</sup>) in the stirring rate in the ultrafiltration cell did not alter the dissolution curve. Measurement of the protein content in the buffer against insulin standards using hplc confirmed that the absorbance was due to insulin. The precision of the dissolution test was estimated using a sample of insulin zinc suspension mixed. On each of six occasions, dissolution curves were obtained for three aliquots from a vial of the insulin sample, using the same stock solution of buffer. The absorbance values at 10 min from the start of each curve were used for calculations. The between- and within-day variability, expressed as a percent coefficient of variation for the absorbance values, were calculated as 11.1% and 9.8% respectively.

Fig. 1 shows the combined dissolution curves for several delayed action insulin formulations, characterized as either a slow, intermediate or fast acting type of insulin. The dissolution curves of all the

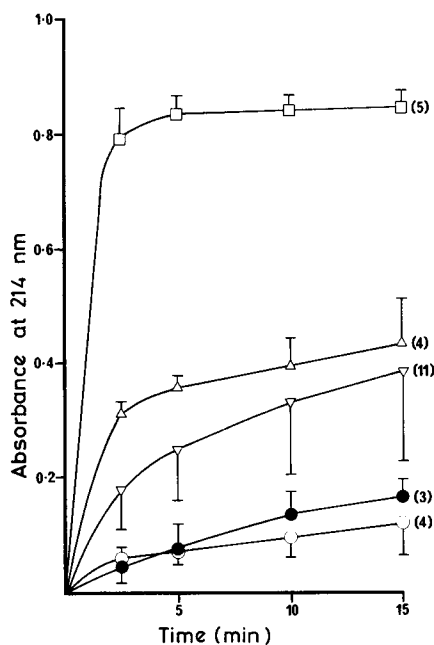


FIG. 1. The combined absorbance curves for each of several insulin formulations. The test measured the dissolution rate of 200 U of the insulin sample into 200 ml of phosphate buffer, pH 7.4, at 37 °C. The standard deviation for each mean is shown and the number of commercial insulin products is given in the brackets. The formulations are: insulin zinc suspension amorphous (□), insulin zinc suspension mixed (Δ), isophane insulin (∇), protamine zinc insulin (●), and insulin zinc suspension crystalline (○).

formulations showed, within the first 5 min, an initial rise of absorbance caused by a relatively rapid release of insulin, followed by a plateau or linear response which was established when most of the insulin crystals had dissolved, as shown by the fast acting, insulin zinc suspension amorphous. The maximum absorbance for 200 U of an insulin solution was 0.850. All the other insulin suspensions gave shallow linear responses rather than a plateau, indicating that insulin was dissolving at a constant rate over the 20 min study period.

Fig. 2 shows the combined hypoglycaemic responses in rabbits produced by the same insulin products that were tested in the in-vitro dissolution test. Although the insulin formulations vary in the rate at which they induce changes in blood sugar concentration, the only statistically significant difference between the curves for the insulin suspensions in the test for prolongation of insulin effect at 6 h was the retardation produced by protamine zinc insulin, which was greater than for the other formulations (Student–Newman–Keul's test,  $P < 0.05$ ). The rabbit test gives variable results. For example the between test coefficient of variation for the mean blood sugar concentration 6 h after injection of

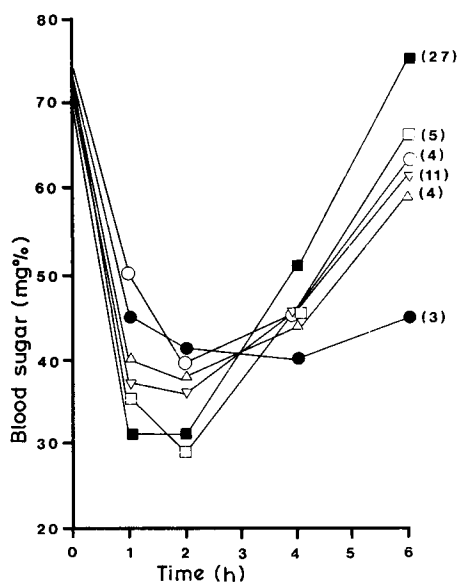


FIG. 2. Hypoglycaemic responses of fasted rabbits to delayed acting insulin formulations. The number of products (or, for the standard insulin solution, the number of tests) is given in the brackets. Each product was tested in 9 rabbits using insulin 5 U kg<sup>-1</sup>. The formulations are: insulin zinc suspension amorphous (□), insulin zinc suspension mixed (Δ), isophane insulin (∇), protamine zinc insulin (●) and insulin zinc suspension crystalline (○). A solution of the 4th International Standard of Insulin (■).



method and either compared directly with a similar insulin reference material or identified in absolute absorbance terms. Thus, 200 U of slow acting insulins could be identified as producing an optical absorbance, at 10 min, of less than 0.2 absorbance units, while the absorbances of 200 U of fast acting insulins exceed 0.8 absorbance units.

The only insulin formulation to show marked variation between products in the in-vitro dissolution test was isophane insulin, some brands of which gave dissolution curves that were closer to those for long acting insulins than for the intermediate types. Since the solubility of the insulin crystals determines the shape of the dissolution curve, factors that can affect the solubility of insulins were examined. These are the species source of the insulin, particle appearance and zinc content (Schlichtkrull et al 1975). Kasama et al (1980) proposed that porcine insulin is more soluble than bovine insulin due to conformational differences between the two. A faster dissolution rate for porcine insulin suspensions would therefore be expected. However, the results of the present study suggest that the particle appearance and not the species source is the most important factor in the dissolution rate of isophane insulin, since bovine and porcine insulin gave similar dissolution rates if their mean particle sizes and shapes were similar. Schlichtkrull et al (1975) showed that the solubility of insulin decreases as the zinc concentration increases. However, at neutral pH and at the concentrations normally present in isophane insulin, zinc ions have little effect on the solubility of the particles. Schlichtkrull et al (1975) found that zinc concentra-

tions above 30 µg/100 U of insulin were needed to reduce the solubility of insulin, which may explain why sample 9, with a high zinc content, gave a slow dissolution rate despite a relatively small particle size.

The results demonstrate that the generic brands of isophane insulin produced by different manufacturers can vary markedly in the dissolution characteristics due largely to differences in particle size and shape. Differences between the isophane products were also indicated by the range for the samples of the mean hypoglycaemic responses in rabbits. The consequence is that, although complying with the BP 1980 requirements for isophane insulin, the different brands may not be bioequivalent. The in-vitro dissolution test offers a means by which the dissolution characteristics of an insulin suspension can be conveniently monitored during both product development and routine manufacture.

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